



MEMS WAFER LEVEL PACKAGING FOR IMPLANTABLE DEVICES

AGENDA / OUTLINE / OVERVIEW

- 1** Introduction
- 2** Wafer level device integration
- 3** Characterization of the packaging
- 4** Coating of the package
- 5** Summary & Conclusions

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“Gradually the electronic devices that were previously external enter in the human body in order to improve therapy or physiological parameter measurements”

Cochlear implants



Medline plus

Brain stimulation



Brain activity sensing

Retina implants

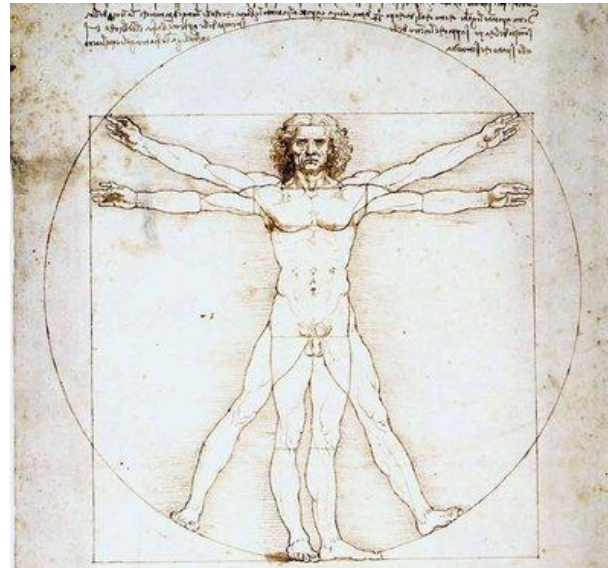


© Inserm, Serge Picaud

Heart Stimulation



Sorin CRM

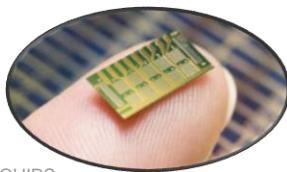


Vagus nerve Stimulation



Europe Orient new

Contraceptif implant



MicroCHIPS.

Localized drug delivery

Bladder Stimulation



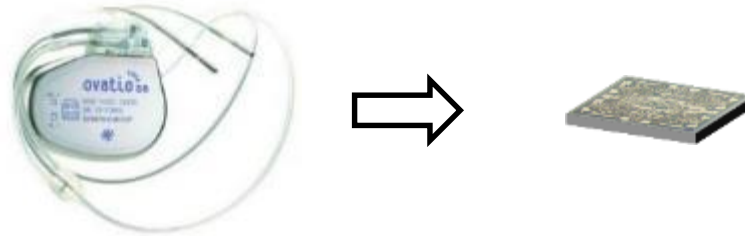
RFID MICROCHIP IMPLANT (HUMAN)



A surgeon implants British scientist Dr [Mark Gasson](#) in his left hand with an RFID microchip (March 16, 2009)

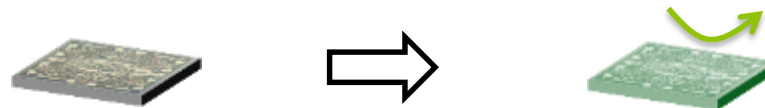
□ Miniaturization

→ Break-through packaging solution: shrink the packaging at the die level



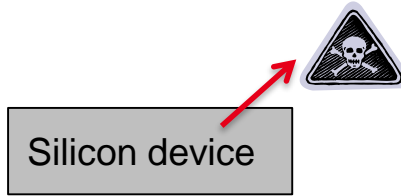
□ Biocompatible encapsulation

→ Need for a diffusion barrier



CHALLENGES OF MEDICAL IMPLANT

Preserve the human body from toxic substances of electronic device



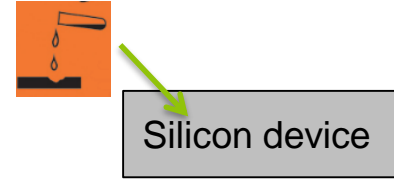
Semiconductor devices are not friendly



bi-directional diffusion barrier needed



Preserve the device from corrosive substances of the human body



Blood plasma has a high concentration of sodium chloride



Multi Barrier recommended



➤ Industrial partner:  **SORIN GROUP** AT THE HEART OF MEDICAL TECHNOLOGY →  **LivaNova**
Health innovation that matters

➤ Application:

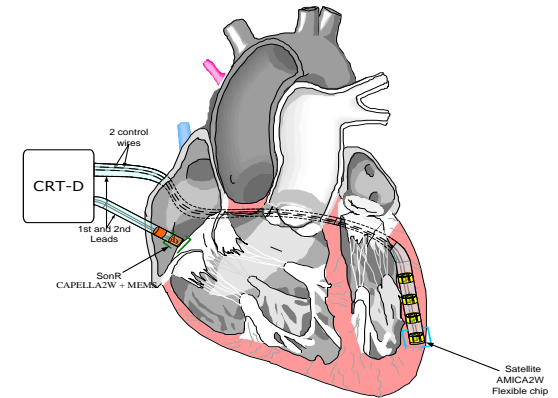
Cardiac implantable device

➤ Objective:

To integrate a MEMS accelerometer and an ASIC chip in cardiac lead in order to sense the endocardial acceleration signal

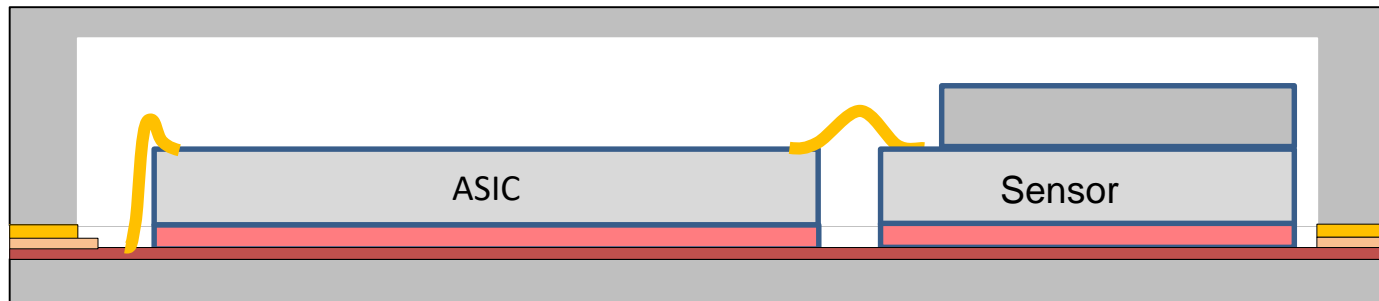
➤ Life target

> 10 years



HERMETIC PACKAGE

Electronics devices are encapsulated in a hermetic box



Hermetic box choices:

- Metal
- Ceramic
- Silicon



LETI ENVIRONNEMENT



**Bio medical
plateform**



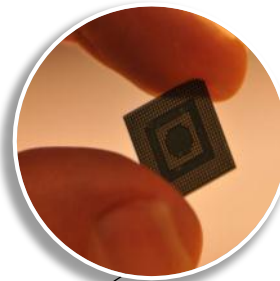
**Chemical &
material
platform**



**Photonic
platform**



**Embedded
systems**



**Micro &
Nanoelectronic
platform**



**Nanocharacterisation
platform**



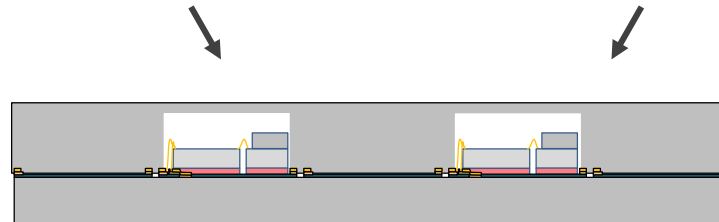
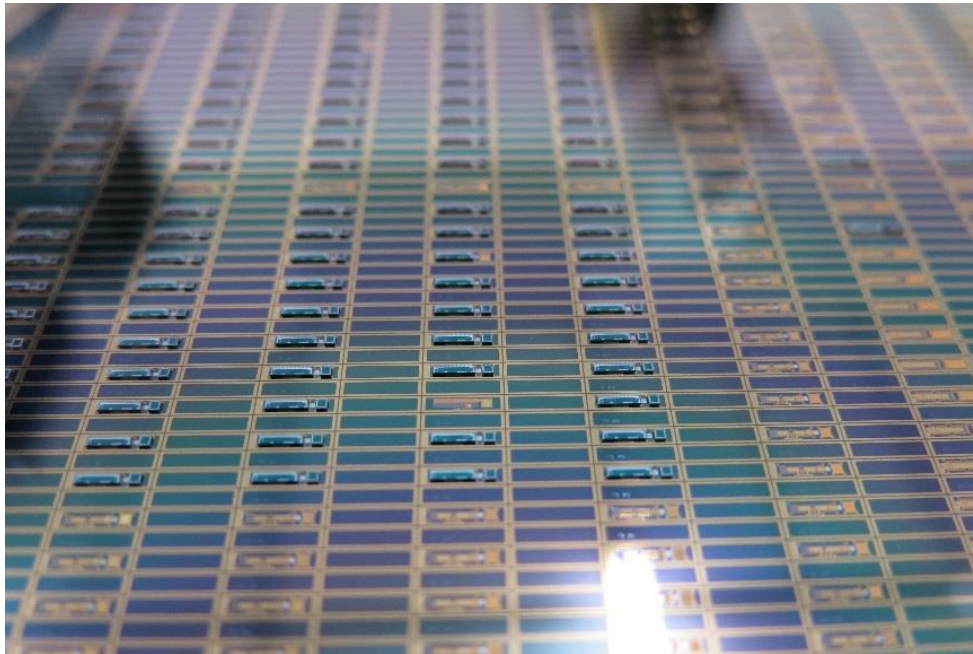
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WAFER LEVEL INTEGRATION

Interposer wafer



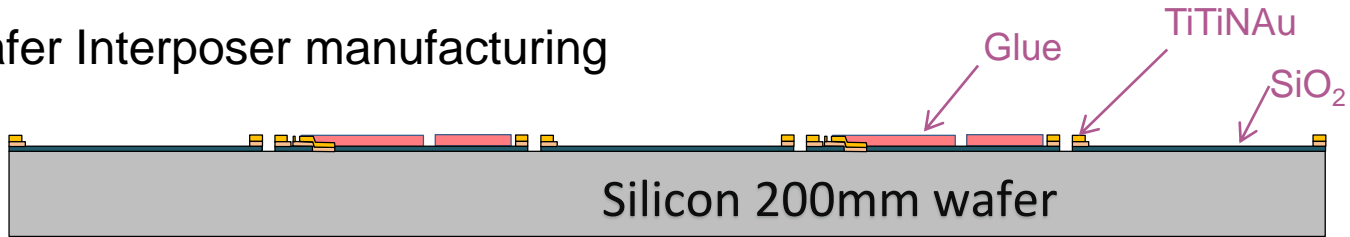
Lid wafer



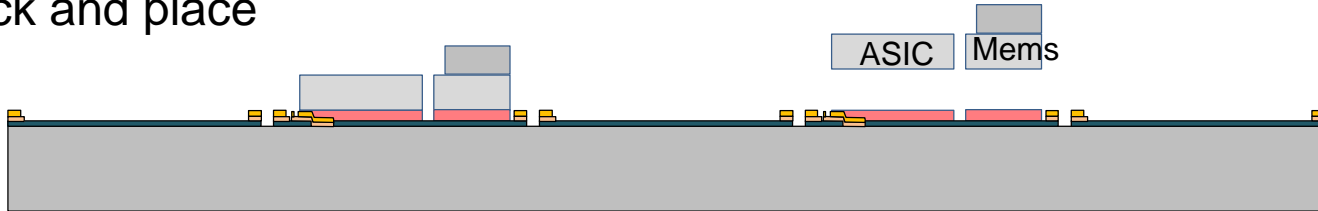
Performed in CEA-LETI clean room

WAFER LEVEL PROCESS FLOW 1/3

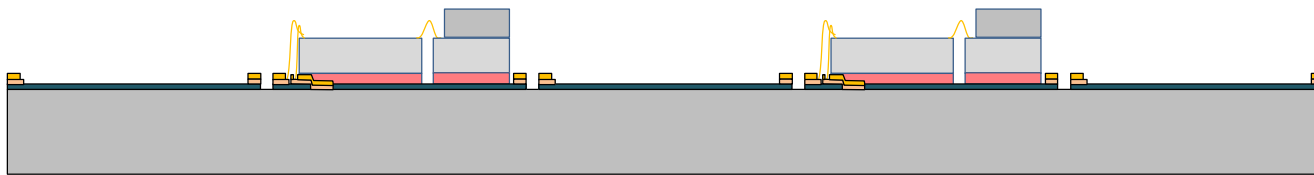
- Wafer Interposer manufacturing



- Pick and place

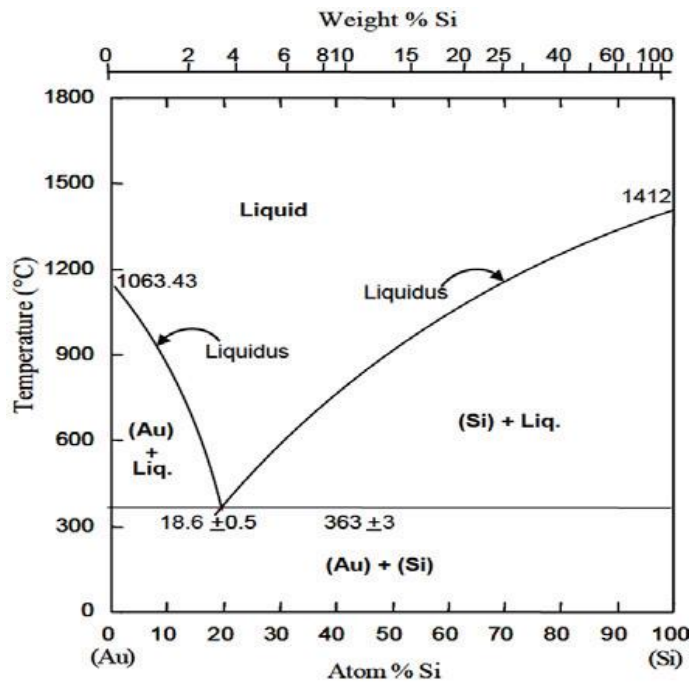
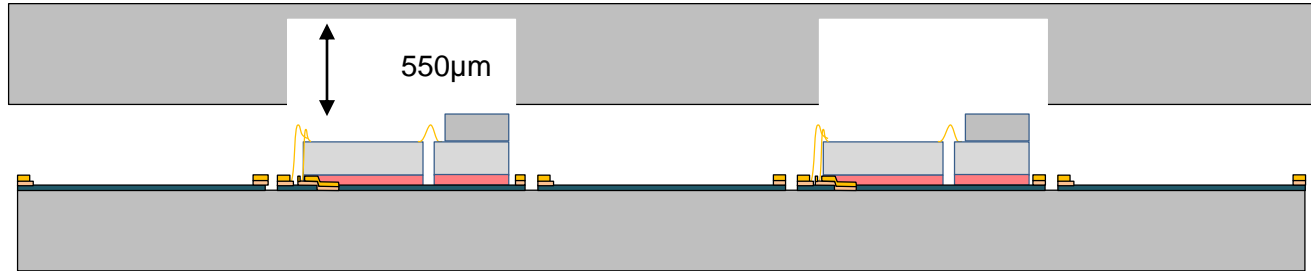


- Wire bonding



- Cavities etching





➤ Lid wafer was bonded to the interposer wafer by eutectic AuSi formation

Bonding conditions:

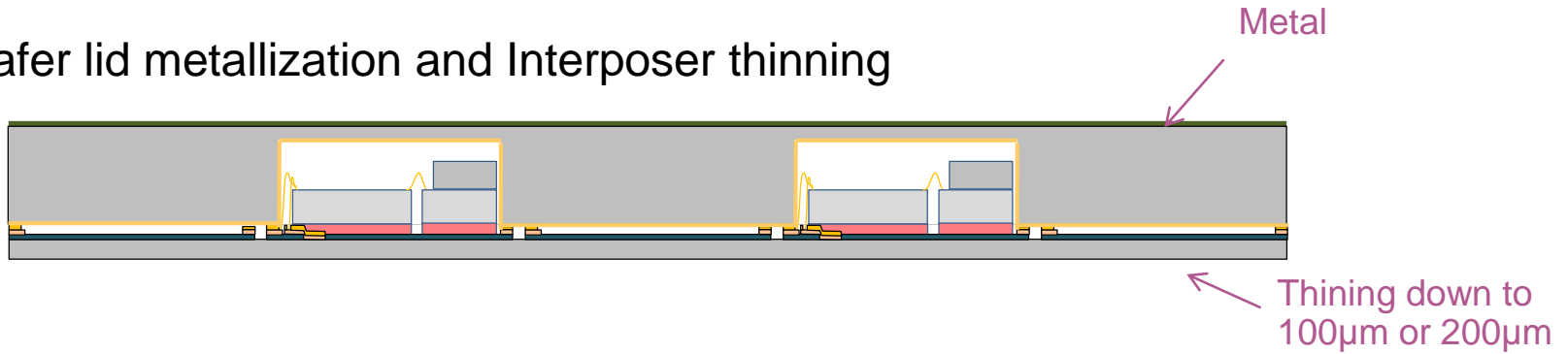
Temperature 400°C,

Pressure = 10000N

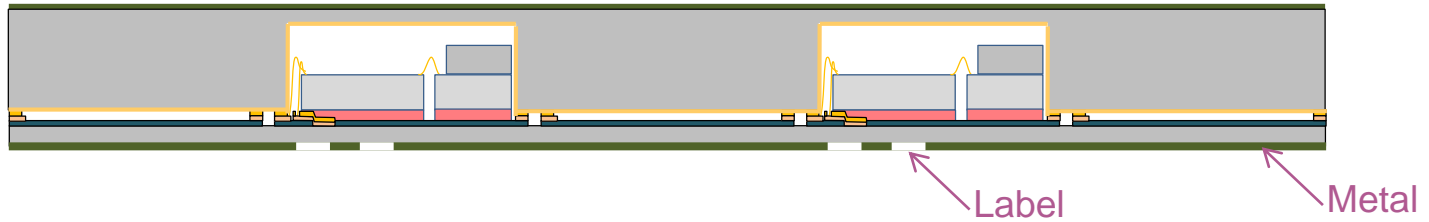
Time = 30 minutes.

Pressure in chamber ~ 5 10⁻³ mbar

- Wafer lid metallization and Interposer thinning



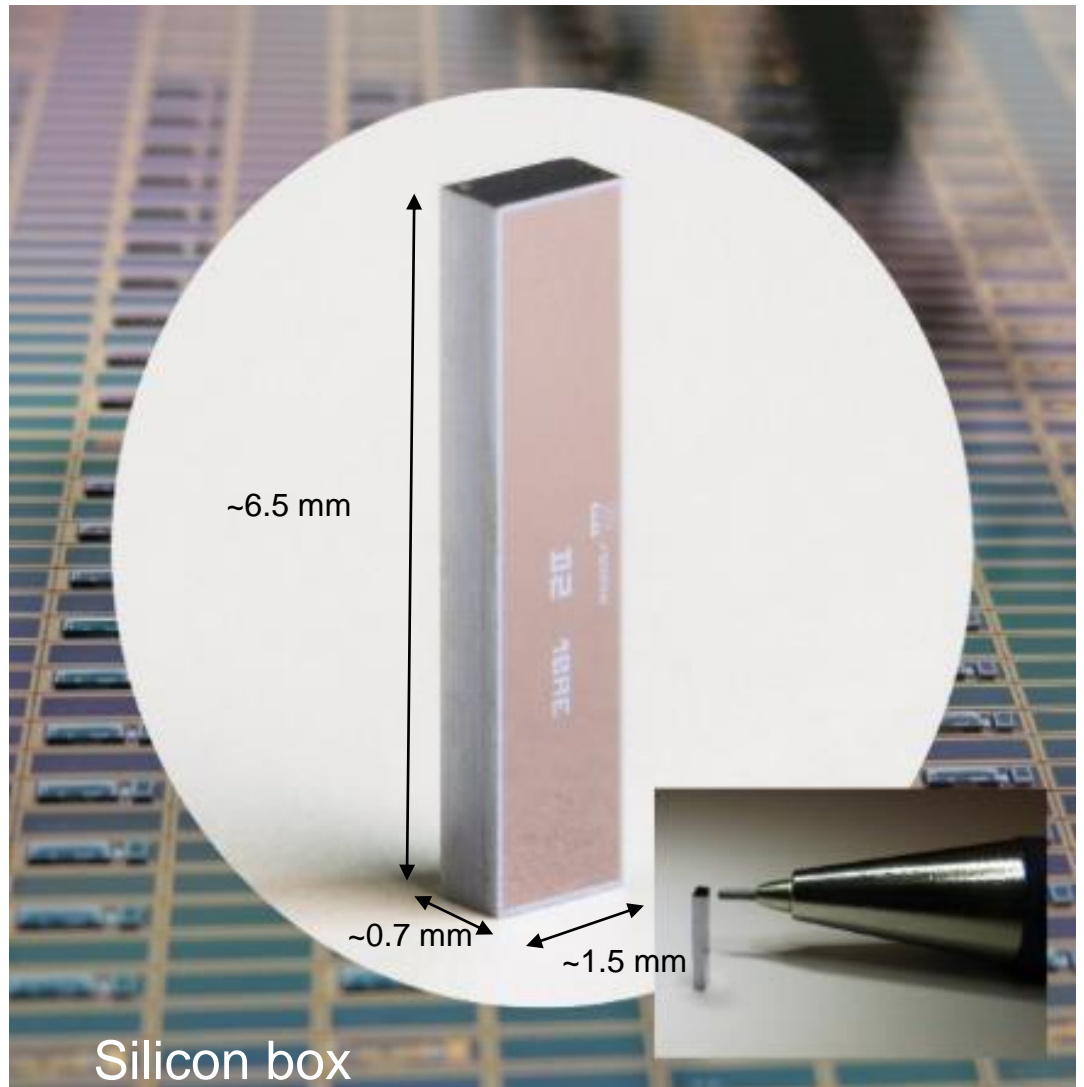
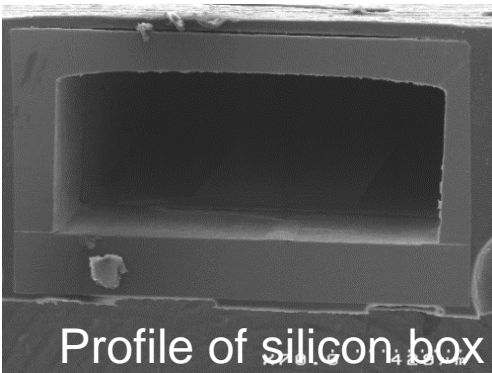
- Metallization and device labeling



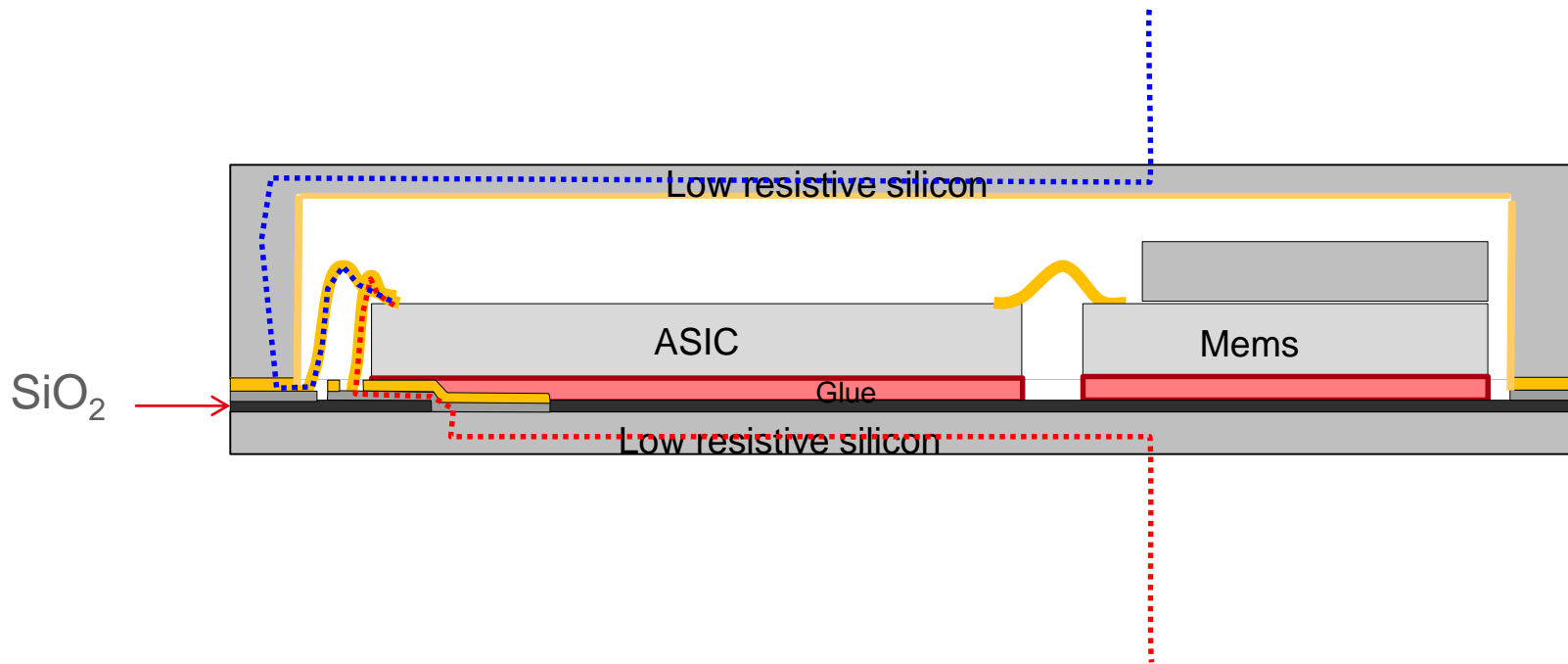
- Dicing



VIEW OF FINAL SILICON PACKAGE



The electrical interconnection to the two conductor wires is obtained through the interposer and the lid using the conductivity of doped silicon (0.1 to 5 mOhm.cm)



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Hermeticity

Residual Gas Analysis

Biostability

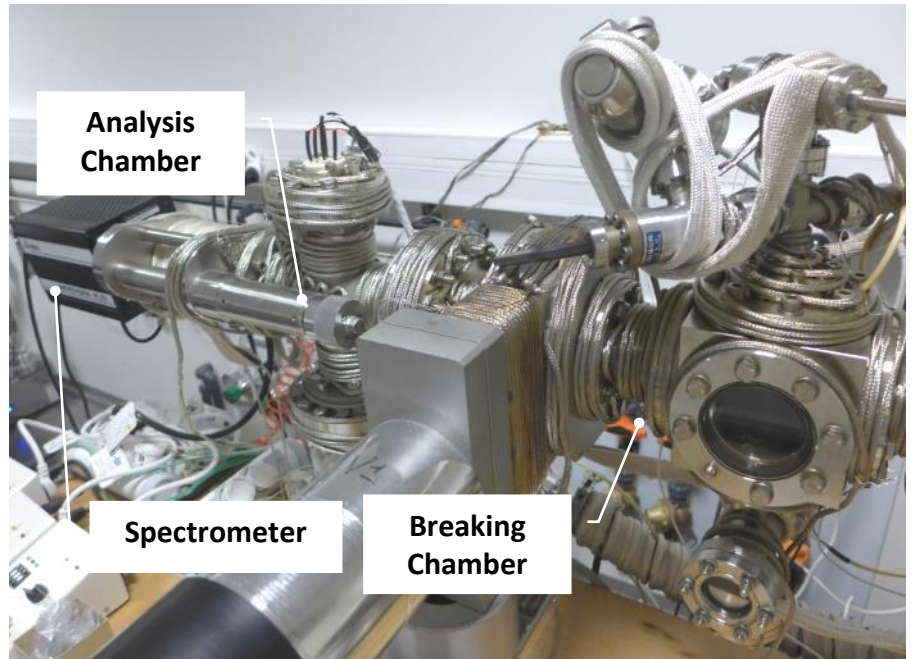
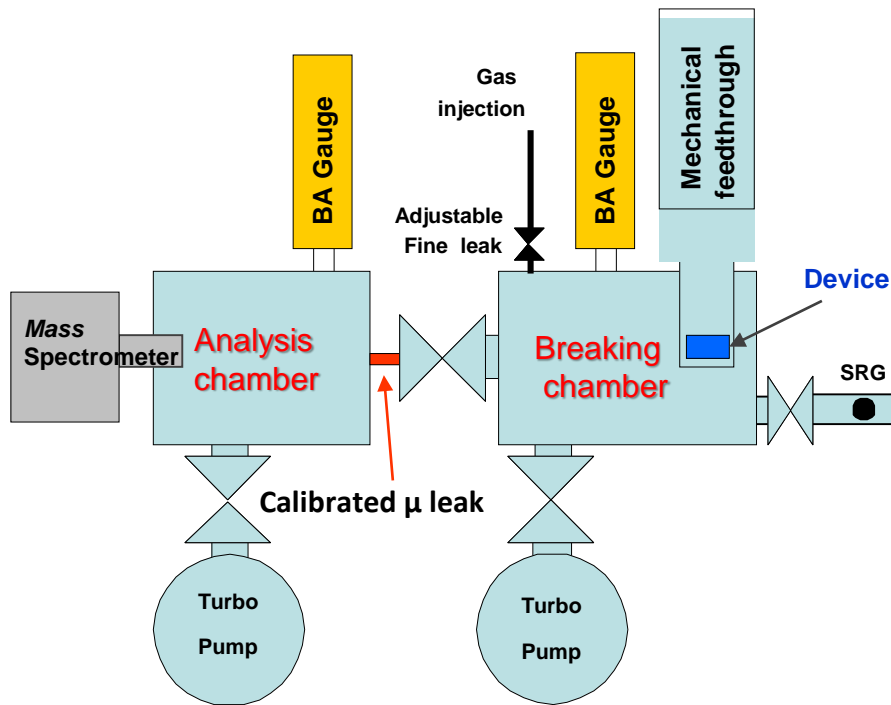
Aging test in Phosphate-Buffered Saline solution

Biocompatibility

In vitro test

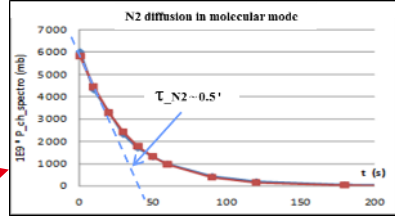
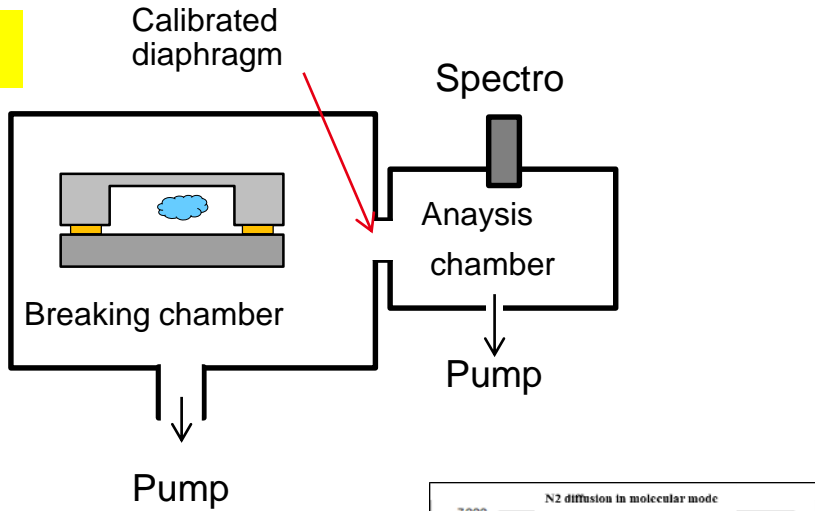
RESIDUAL GAZ ANALYSIS

Specific tools has been developped in CEA-LETI to analyse small amount of gases inside low volume at low pressure (1mm^3 , 10^{-3} mb -> $4 \cdot 10^{-14}$ moles)

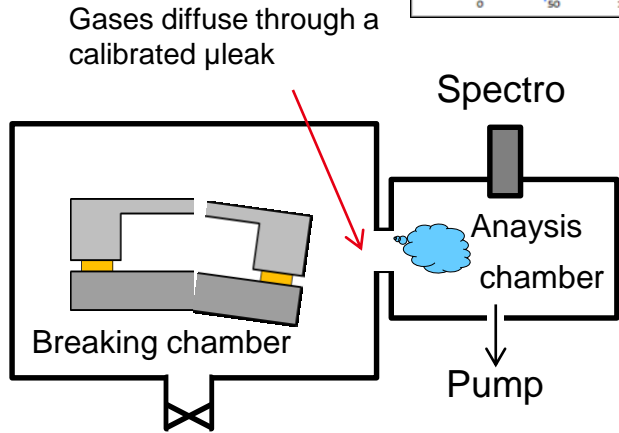


RGA PROCEDURE

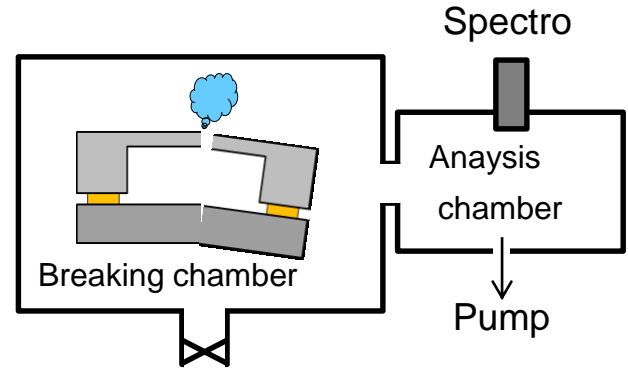
1



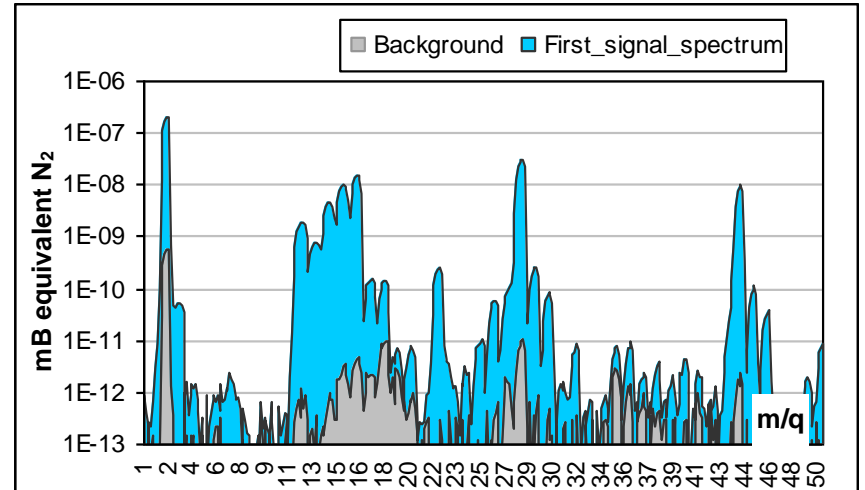
3

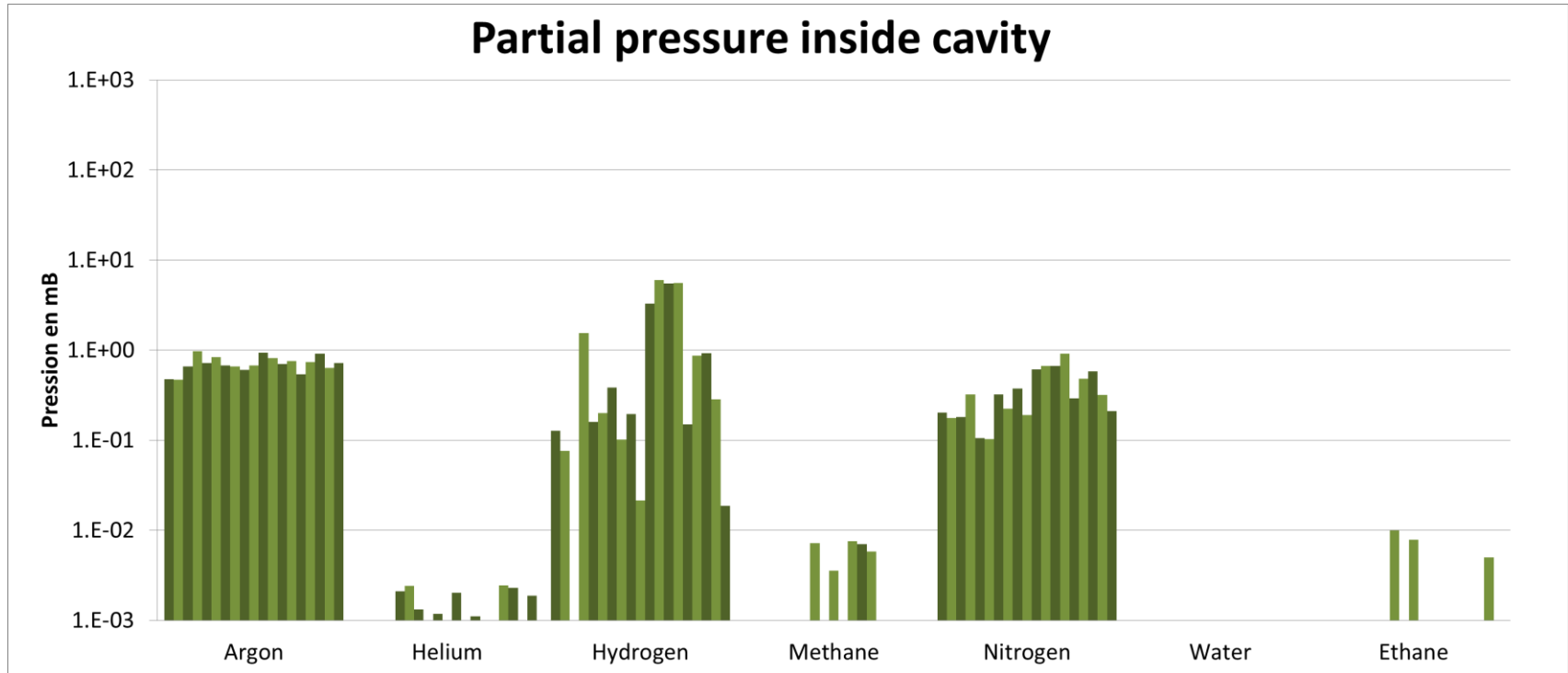


2



Typical spectrogram performed during an RGA experiment

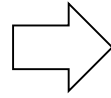
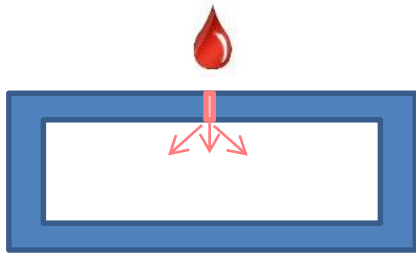




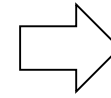
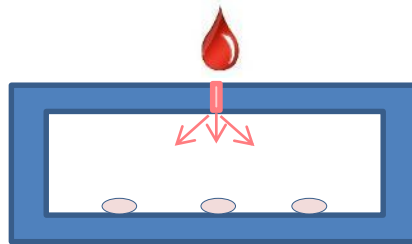
- Total pressure < 10 mbar
- Homogeneous results for Ar but large dispersion for H₂
- Origins of Gas detected: entrapped in materials during process deposition, surface preparation or bonding procedure

CAUSE OF FAILURE

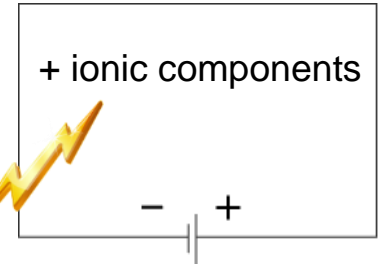
Leak



Drop formation in cavity



Corrosion → Risk of short circuit



Recommandation during the life time



"To be below the dew point in the cavity"



$$P_{H_2O} < 0.062 \text{ atm à } T=37^{\circ}\text{C}$$



$$P_{H_2O} < 0.052 \text{ atm à } T=37^{\circ}\text{C}$$

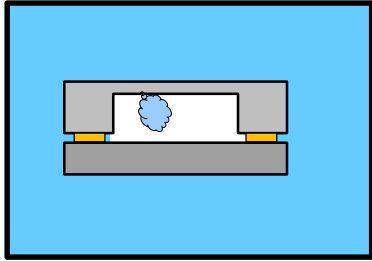


$$L_{H_2O} < 1.2 \cdot 10^{-12} \text{ atm.cc/s}$$



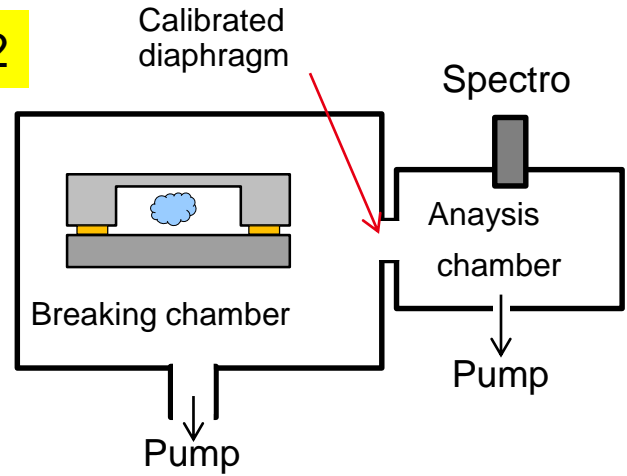
LEAK RATE EVALUATED USING RGA

1

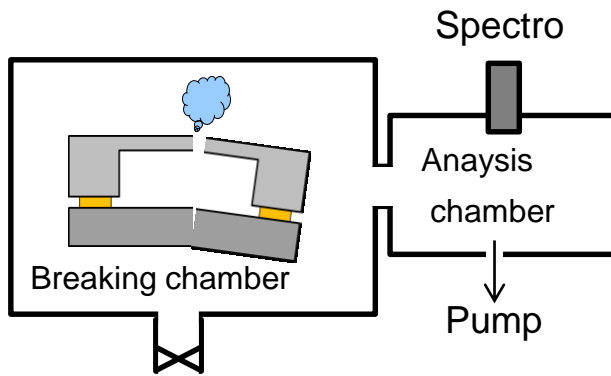


Pressurization with C₂H₆ (P,time).

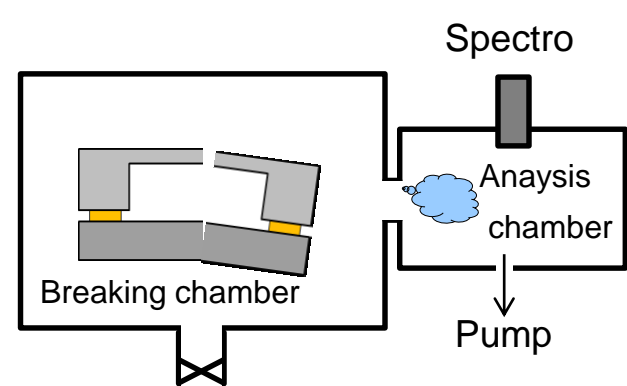
2



3



4



$$\Delta P t = \Delta P_0 e^{\frac{-L t}{V P_0}}$$

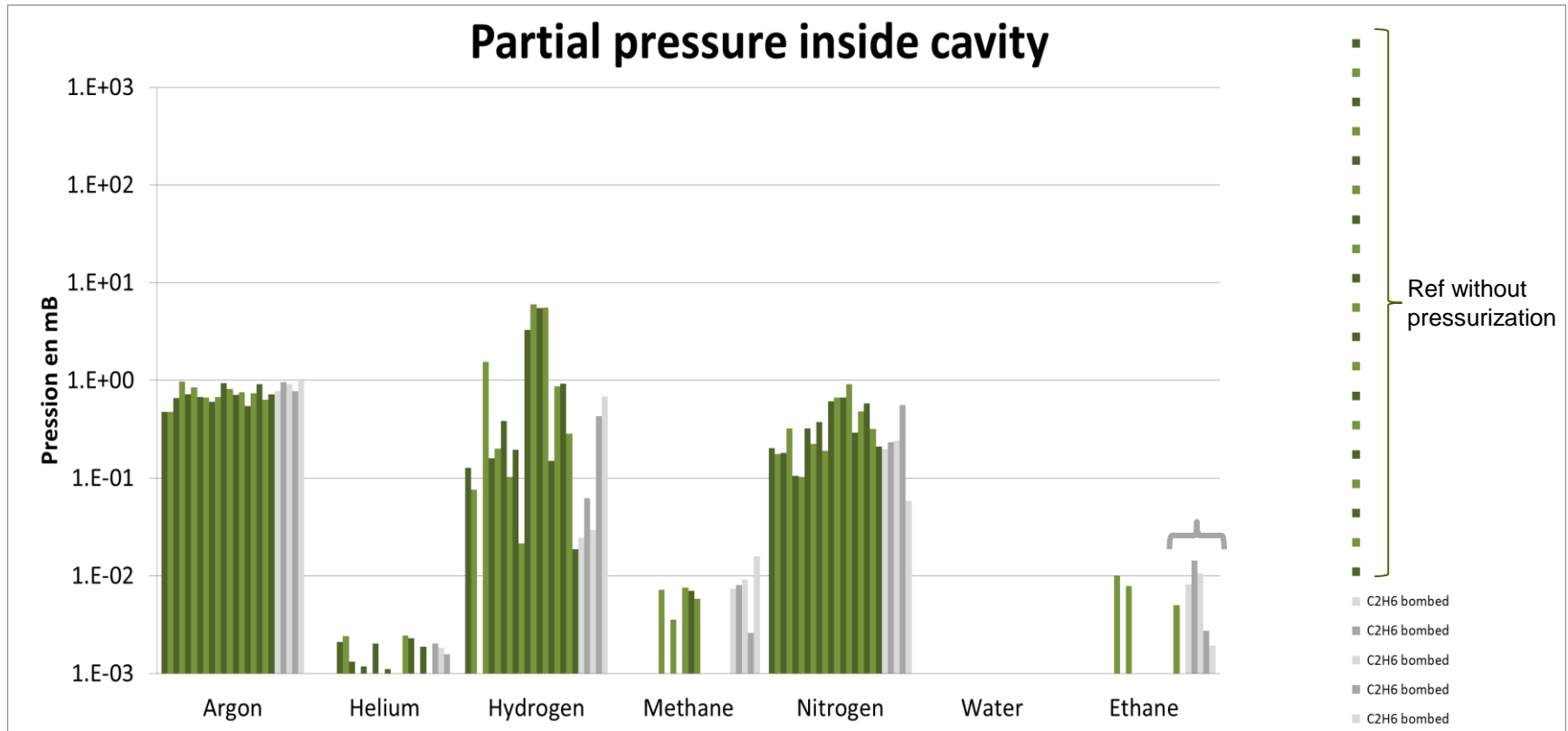


$$L_{C_2H_6}$$



$$L_{H_2O} = L_{C_2H_6} \times \sqrt{\frac{M_{C_2H_6}}{M_{H_2O}}}$$

EXAMPLE OF RGA RESULTS ON DEVICES AFTER PRESSURIZATION WITH ETHANE



- The Ethane is always present after pressurization but values are closed to the limit of detection

$$L_{H_2O} < 1 \cdot 10^{-15} \text{ atm.cc/s}$$

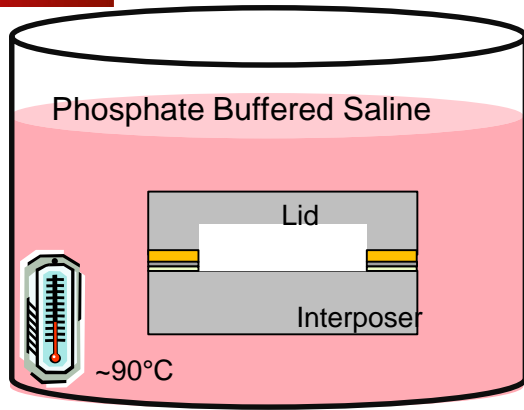
- The water standard leak rate was estimated to $<1 \cdot 10^{-15}$ atm.cc/s for bonding ring of TiTiN/Au
- These leaks guarantee a life time much more than 20 years ($L_{\text{H}_2\text{O}} < 1.2 \cdot 10^{-12}$)

What about biostability ?

Packaging was tested in Phosphate-buffered saline

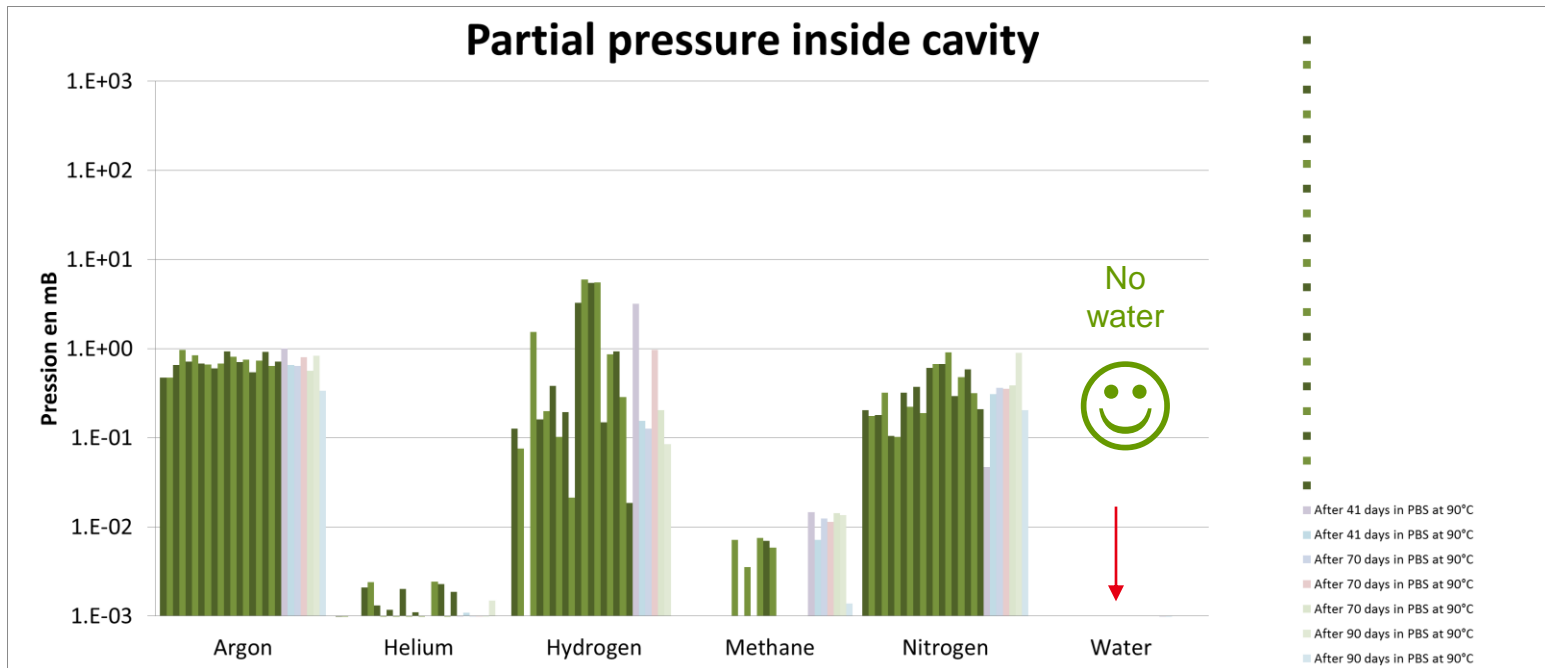
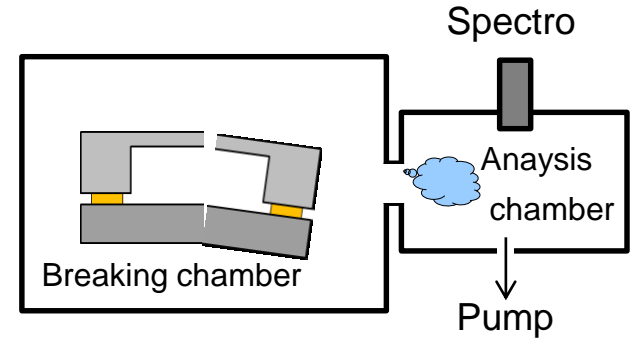
Phosphate-buffered saline (abbreviated PBS) is a water-based salt solution which the osmolarity and ion concentrations of the solutions match those of the human body (isotonic).

BONDING RESISTANCE IN SALINE SOLUTION



After
41, 70 and 90 days

RGA analysis



What about biocomp ?

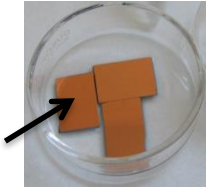
Biological Evaluation of MDs : ISO 10993

Device Category		Biological Effect										
		In-vitro		In-vivo								
		Cytotoxicity	Sensitization	Irritation or Intracutaneous Reactivity	Systemic Toxicity (Acute)	Sub-chronic Toxicity (Sub-acute Toxicity)	Genotoxicity	Implantation	Hemocompatibility	Chronic toxicity	Carcinogenicity	
Body Contact	Contact duration											
	A – Limited (≤ 24 h)											
	B – Prolonged (24 h to 30 days)											
	C – Permanent (> 30 days)											
Implant devices	Tissue/bone	A	X	X	X	O						
		B	X	X	O	O	O	X	X			
		C	X	X	O	O	O	X	X		X	X
	Blood	A	X	X	X	X			X	X		
		B	X	X	X	X	O	X	X	X		
		C	X	X	X	X	X	X	X	X	X	X

PROTOCOL FOR TEST ON EXTRACTS



Extracts preparation
(materials)

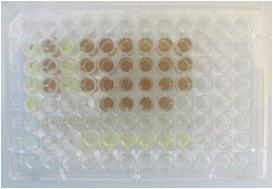
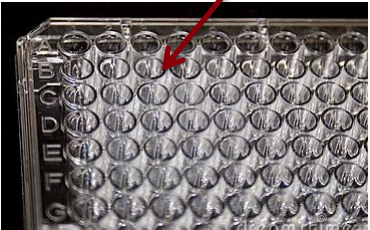
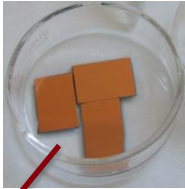


Incubation of extracts
With L929 cells

Cell viability assessment



L929 cells seeding



$$\text{Percent viability} = \frac{100 \times \text{OD}_{c492e}}{\text{OD}_{c492rc}}$$

RESULTS OF CELL VIABILITY

Material	Percent viability of control	System suitability
Positive control (Polyurethane film with ZDEC)	8,6	Met criteria
Negative control (High density Polyethylene)	100	Met criteria

Material	Percent viability of tested materials	Cytotoxic potential
Doped Si wafer	100	No cytotoxic potential 😊
Doped Si wafer / Ti/TiN	100	No cytotoxic potential 😊

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BIO PACKAGING LAYER

Interest ↑

Material	Fabrication	Biocomp. (L929)	Biostable (PBS 37°C)
TiO ₂	ALCVD 250°C	Yes	Yes
Al ₂ O ₃	ALCVD 250°C	Yes	Yes
HfO ₂	ALCVD 250°C	Yes	Yes
SiC	PECVD 350°C	Yes	Yes
SiOC	PECVD 400°C	Yes	Yes
DLC (a-CH)	PECVD 400°C	Yes	Yes
BN	PECVD 400°C	Yes	Yes
SiO ₂	PECVD 400°C	Yes	Medium
SiN	PECVD 400°C	Yes	No
crys-ZnO	ALCVD 250°C	No	No

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- ❑ A new packaging solution of an ASIC and MEMS for cardiac medical applications was presented.
 - Low profile silicon box manufacturing was demonstrated
- ❑ The gas content and hermeticity of the package were analyzed using Residual Gas Analysis
 - The water standard leak rate was estimated to $<1 \text{ } 10\text{-}15 \text{ atm.cc/s}$ which guarantees a life time much more than 20 years.
- ❑ Our packaging has presented a good resistant to PBS ($>3\text{months}$ at 90°C)
- ❑ Cytotoxicity and cell morphology test protocols according to the norm ISO-10993 were developed.
- ❑ Good candidates as additional biopackaging layer were identified

Thanks
for your attention

Leti, technology research institute

Commissariat à l'énergie atomique et aux énergies alternatives
Minatec Campus | 17 rue des Martyrs | 38054 Grenoble Cedex | France
www.leti-cea.com

